

Introduction

- VMAT machine parameter optimization (MPO)**, or setting MLC positions and monitor units (MUs) at every control point of an arc, is a high-dimensional, constrained problem solved by inverse planning that is sensitive to objective and weight choices, driving long, variable planning times.
- These limits are acute** in online adaptive and real-time radiotherapy, where plans must be re-optimized rapidly to daily anatomical change.
- Supervised learning** still relies on a conventional optimizer and is bounded by training-plan quality. Reinforcement learning (RL) instead maximizes a reward, giving it the ability to discover novel solutions and generalize across clinical goals.
- Prior RL work** either tuned TPS parameters as a “virtual planner” or still invoked a commercial TPS in the final stage to reach clinical quality.

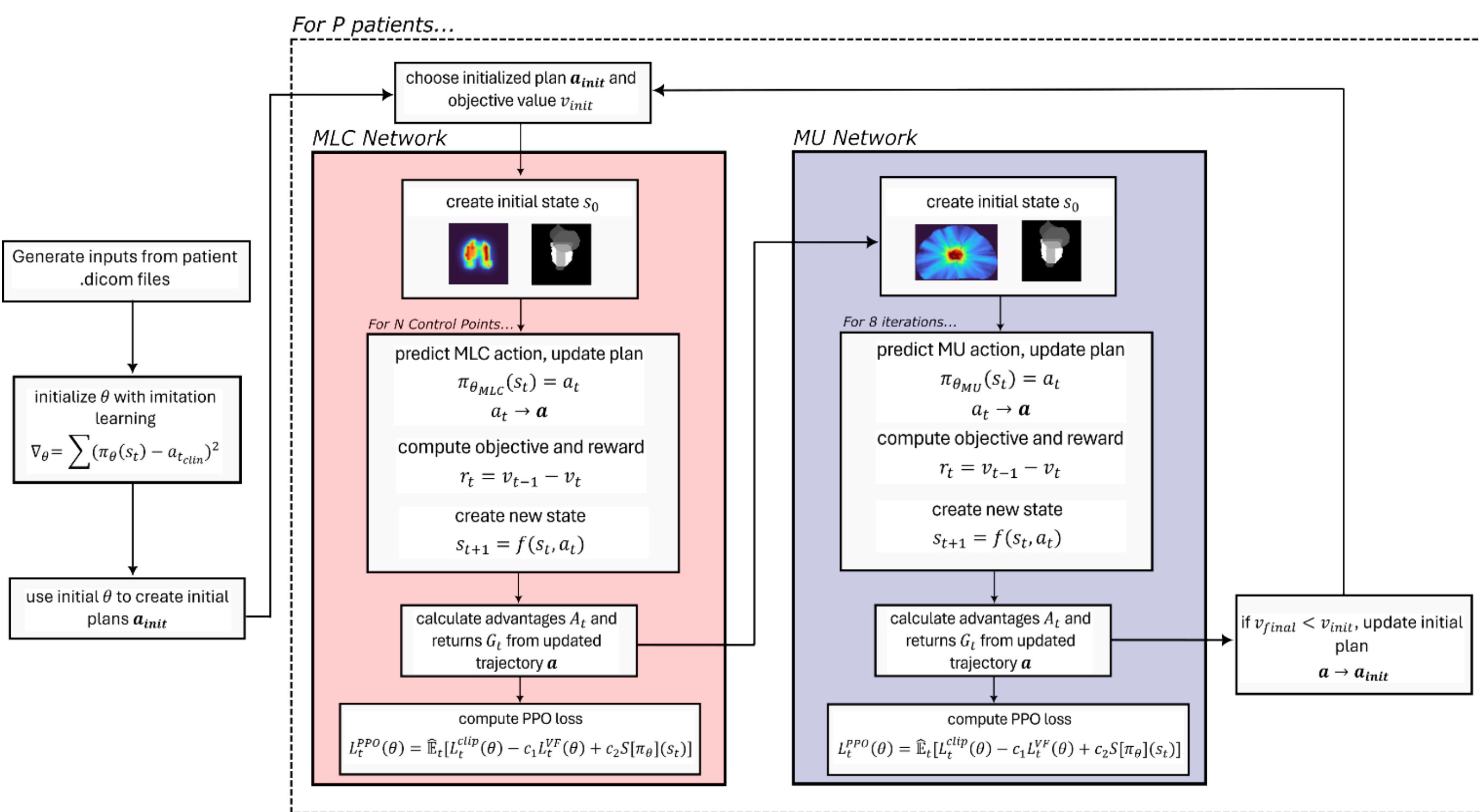


Figure 1. Training workflow with sequential RL updates of the tandem MLC and MU networks.

Purpose

- Develop and validate** a deep-RL VMAT MPO algorithm that automatically generates clinically comparable prostate cancer plans meeting machine constraints while being entirely independent of a commercial TPS optimizer.

Methods & Materials

- Cohort:** 100 prostate SBRT patients (PACE-B), 36.25 Gy / 5 fx, 5 mm PTV margin, 70/10/20 training / validation / testing split. Elekta Unity MR-Linac VMAT in a research Monaco build; single arc, 2° control points, 4–23° cryostat gap; in-house developed dose calculation[1].
- MDP:** VMAT MPO cast as a finite Markov decision process (MDP) over N control points; the policy maps state $s_t \rightarrow$ next machine parameters, earning a DVH-based reward r_t .
- Tandem CNNs:** a spatial MLC network (per control point, BEV inputs) and a global MU network (all control points). Decoupling MLC / MU exploration stabilized training.
- Reward:** per-structure mean square error (MSE) to ideal dose, scaled down each time a constraint is met, driving the agent to meet clinical objectives.
- Training:** Proximal policy optimization (PPO) actor–critic (clip $\epsilon = 0.15$) + GAE ($\gamma = 0.99$, $\lambda = 0.95$); imitation-learning warm start; TensorFlow 2.12 on 8× Tesla V100.

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[1] Shaffer N, Snyder J, St-Aubin J. Validation of a rapid algorithm for repeated intensity modulated radiation therapy dose calculations. *Biomed Phys Eng Express*. 2024;11(1):015046.

[2] Shaffer N, Mudireddy AR, St-Aubin J. A tandem reinforcement learning framework for localized prostate cancer treatment planning and machine parameter optimization. *Medical Physics*. 2026;53(2):e70306.

Results

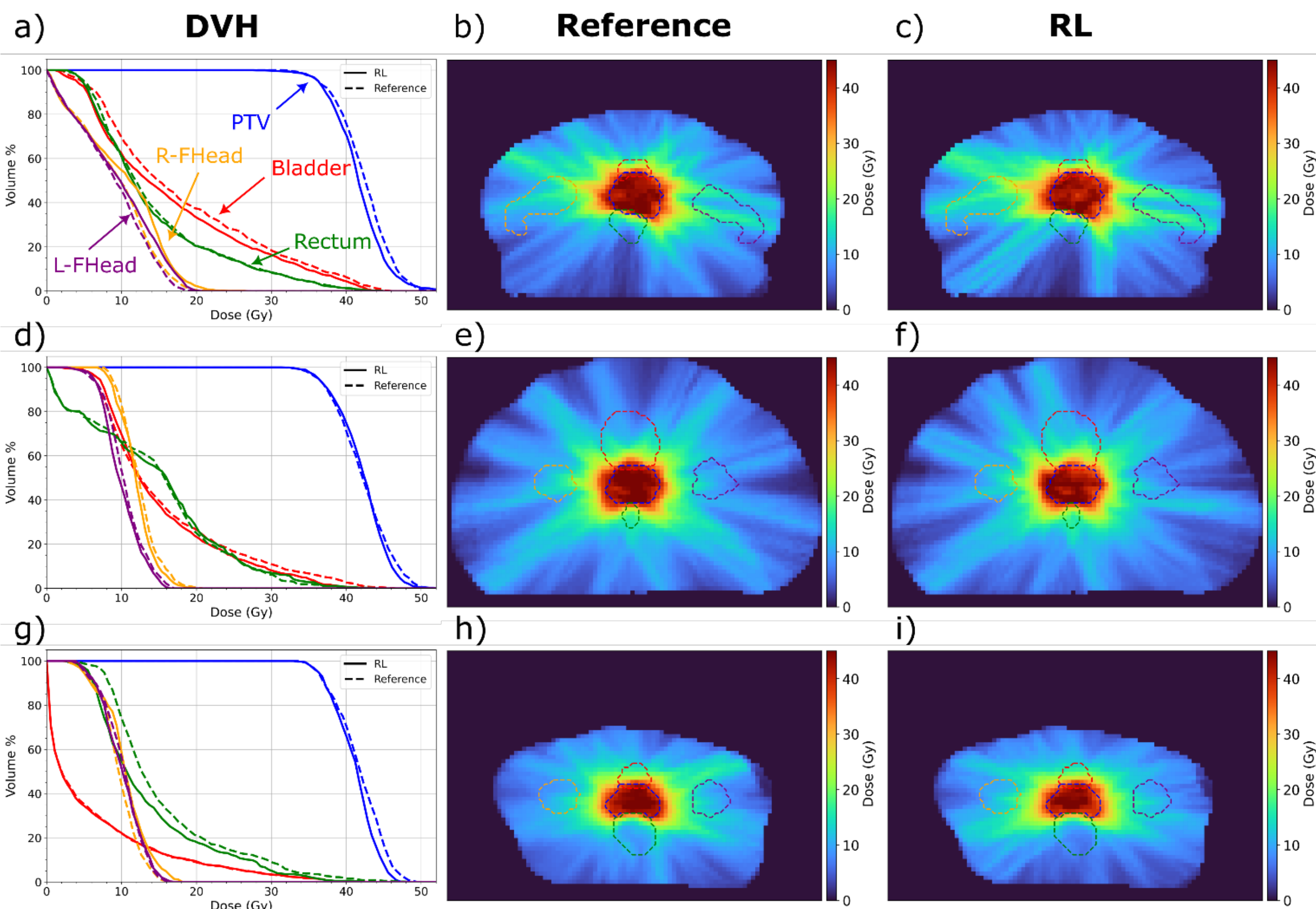


Figure 2. DVHs (a, d, g) with axial reference (b, e, h) and RL (c, f, i) dose distributions for three sample patients. Contours: PTV (blue), bladder (red), rectum (green), R/L femoral heads (orange/purple).

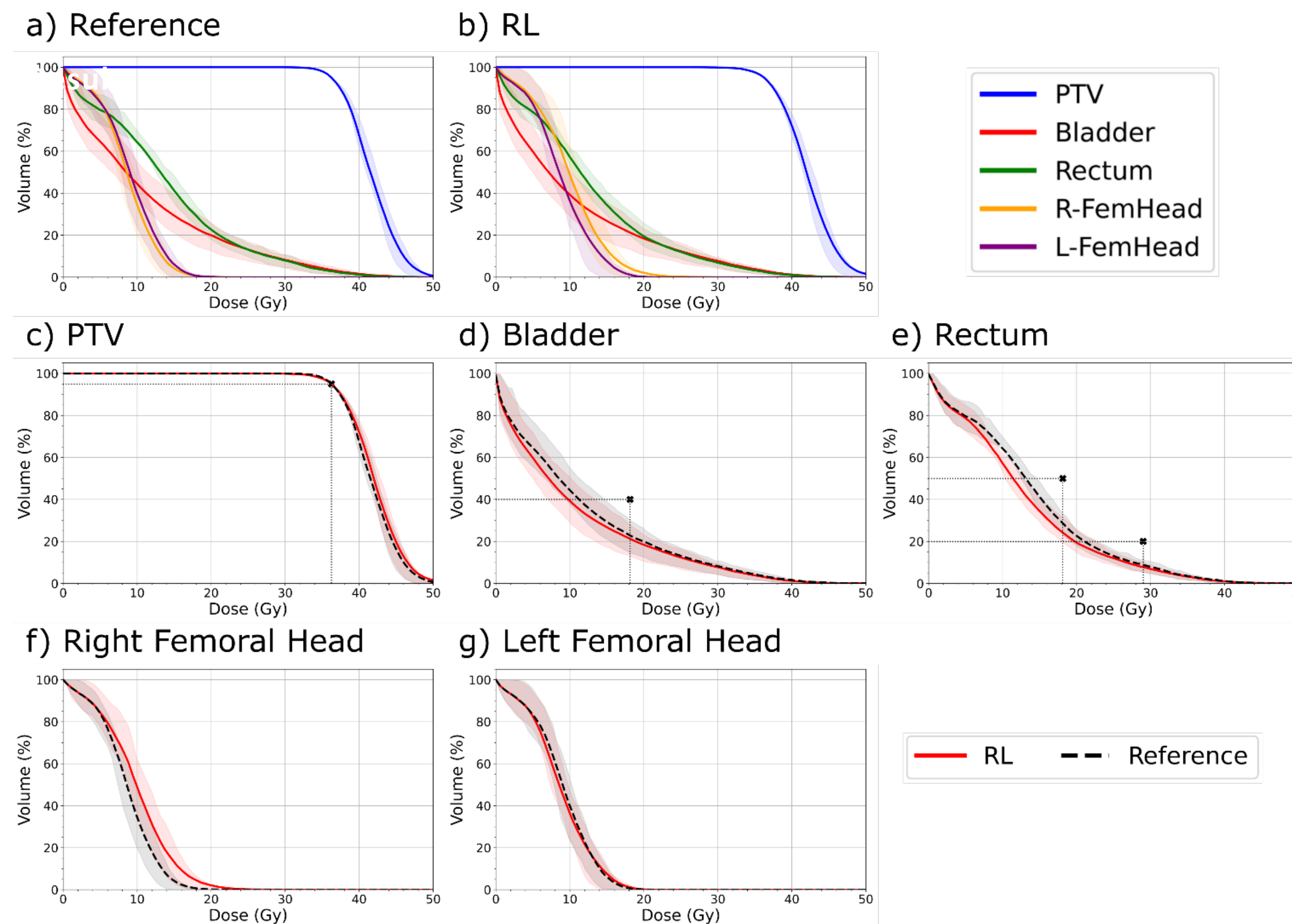


Figure 3. Mean DVH for reference (a) and RL (b) plans, with per-structure curves (c–g). Black markers denote reward constraints; shaded bands show the interquartile range.

Table 1. Mean $\pm$ SD dose metrics for reference vs. RL plans (test cohort). Significant differences ($p < 0.05$) in bold*.

Structure	Metric	Reference	RL	p
PTV	Dmean (Gy)	41.64 $\pm$ 1.23	42.01 $\pm$ 1.22	0.304
	D2% (Gy)	47.35 $\pm$ 2.61	48.10 $\pm$ 2.50	0.048*
	D98% (Gy)	34.94 $\pm$ 0.60	34.59 $\pm$ 0.67	0.224
	CI	1.40 $\pm$ 0.11	1.42 $\pm$ 0.07	0.251
Bladder	Dmean (Gy)	11.41 $\pm$ 3.99	10.58 $\pm$ 3.75	0.417
	V50% (Gy)	8.29 $\pm$ 3.79	7.71 $\pm$ 3.45	0.607
Rectum	Dmean (Gy)	14.04 $\pm$ 2.13	12.96 $\pm$ 1.85	0.020*
	V50% (Gy)	10.41 $\pm$ 3.14	8.79 $\pm$ 2.74	0.130
	V80% (Gy)	3.18 $\pm$ 1.53	2.83 $\pm$ 1.32	0.417
L Fem. Head	Dmean (Gy)	8.92 $\pm$ 1.65	8.72 $\pm$ 1.87	0.626
	V40% (Gy)	2.85 $\pm$ 2.48	3.39 $\pm$ 3.64	0.892
R Fem. Head	Dmean (Gy)	8.57 $\pm$ 1.74	9.87 $\pm$ 2.24	0.045*
	V40% (Gy)	1.97 $\pm$ 2.62	5.59 $\pm$ 5.11	0.020*

6.3s

avg. plan generation

100%

of RL plans met all clinical constraints

- Fast auto-planning:** RL plans were generated in 6.3 ± 4.7 seconds
- Adaptive inference:** plans used variable amount of inference passes, continuing while total plan quality continued to improve
- Clinically comparable:** all plans met every pre-defined planning objective
- Improved OAR sparing:** RL plans had improved bladder and rectum sparing vs. reference plans
- All plans are physical:** plans are all in agreement with the machine’s mechanical limits (425 MU/min, 6 cm/s leaf speed).

Discussion

- End-to-end RL VMAT MPO** produces clinically acceptable prostate SBRT plans in ~ 6 s with no commercial optimizer
- Constraint-driven reward** taught the agent to meet clinical goals without using clinical plans for training; OAR weighting may be slightly over-prioritized vs. PTV homogeneity but is tunable for future iterations of this work.
- Future Work:** multi-arc plans for higher-risk disease; geometric rewards for avoidance angles; variable dose rate; finer 2–3 mm dose grids; GPU-side pre-processing; DICOM-RT export once Unity import is supported.

Conclusion

- Built a deep-RL framework** for end-to-end VMAT optimization rapidly generates prostate SBRT plans that are dosimetrically comparable to conventional plans and meet all machine constraints without a commercial TPS optimizer.
- Its speed, adaptability, and independence** from prior plan quality make it a promising auto-planning tool for adaptive radiotherapy.

*Since submission, this work was published in *Medical Physics* [2]