

Introduction

Deep-learning auto-segmentation is increasingly used in radiotherapy to reduce contouring time and inter-observer variability but must be validated before clinical adoption. This study validates a commercial system (MVision AI) against clinical contours across head-and-neck and prostate cohorts using geometric and dosimetric endpoints and examines the suitability of different performance metrics for different contours.

Method

MVision AI auto-contours were compared against approved clinical contours across two sites. Cohort, metrics, and acceptance thresholds are given in **Table 1**. Dosimetric agreement was assessed by recomputing dose on the AI and clinical contours from the same clinical plan, with no re-optimisation, so differences reflect only contour geometry.

Table 1. Cohort characteristics, geometric and dosimetric metrics, and clinical acceptance thresholds.

	H&N	Prostate
Patients	15	15
Slice thickness	1.25-3.0mm	1.25-3.0 mm
Metric	Type	Threshold
DSC	Volume overlap	≥ 0.80
s-DSC (τ = 3 mm)[1]	Boundary	≥ 0.85
Mean, D2, D95, D98	Dose difference	—

Results

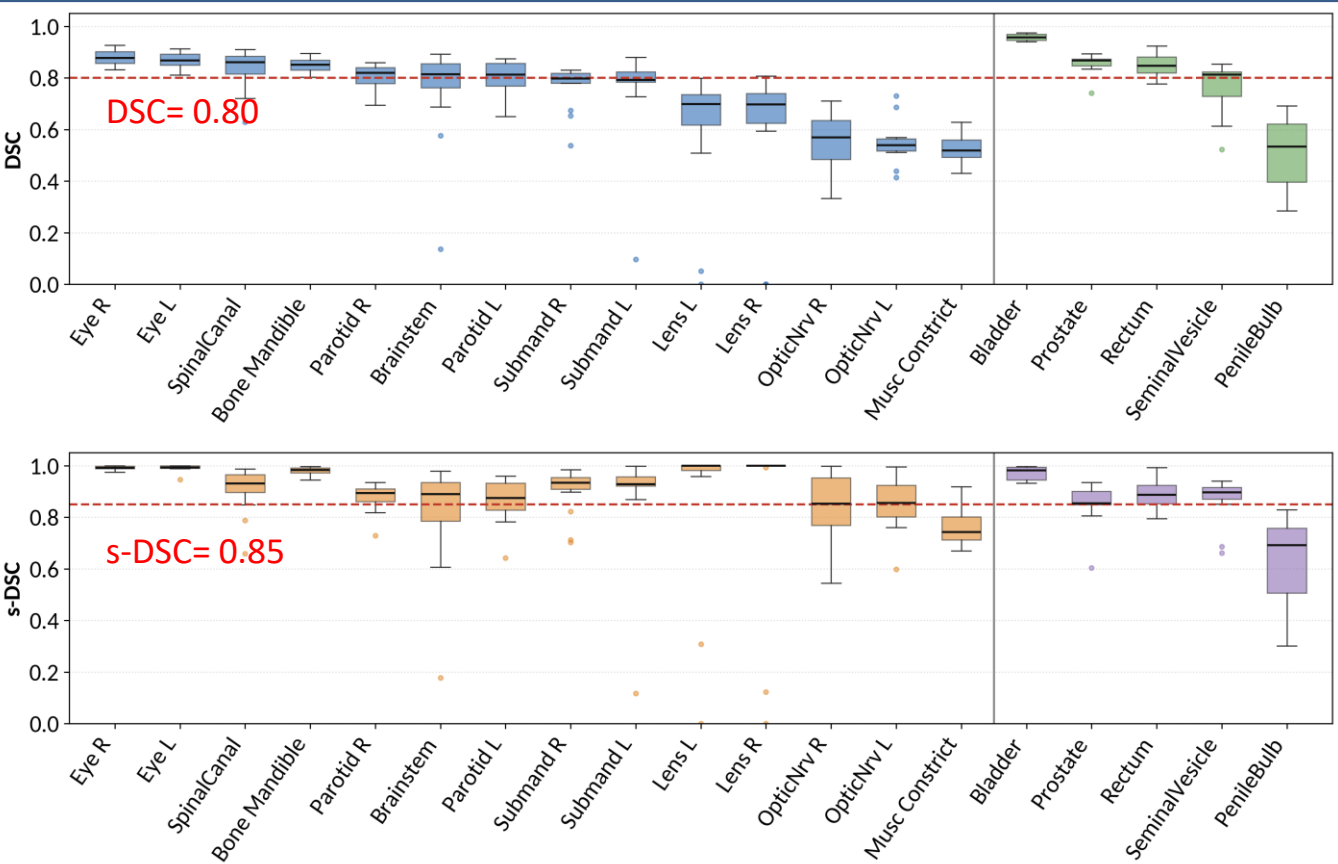


Figure 1. Geometric agreement between MVision AI and clinical contours, shown as DSC (top) and surface DSC ($\tau = 3$ mm, bottom). Small structures (lens, optic nerves) fall below the DSC threshold while remaining above the surface-DSC threshold, illustrating that the choice of metric changes the acceptance outcome for these structures.

Take Home Message

- MVision is clinically acceptable for most OARs.** Median DSC 0.52–0.96; s-DSC ≥ 0.85 for all structures except muscle constrictor and penile bulb (**Fig 1**).
- The two metrics diverge for small organs.** Disagreements concentrate in contours < 10 cc (median 1.3 cc); larger organs agree (**Fig 2**).
- DSC's rejection has no dosimetric basis.** Contours DSC rejected but s-DSC accepted differ by only 0.15 Gy (2.8%) mean / 0.09 Gy (1.1%) near-max (**Table 2**).
- Use s-DSC for small OARs** — DSC's volume-overlap is disproportionately penalised at low volume.

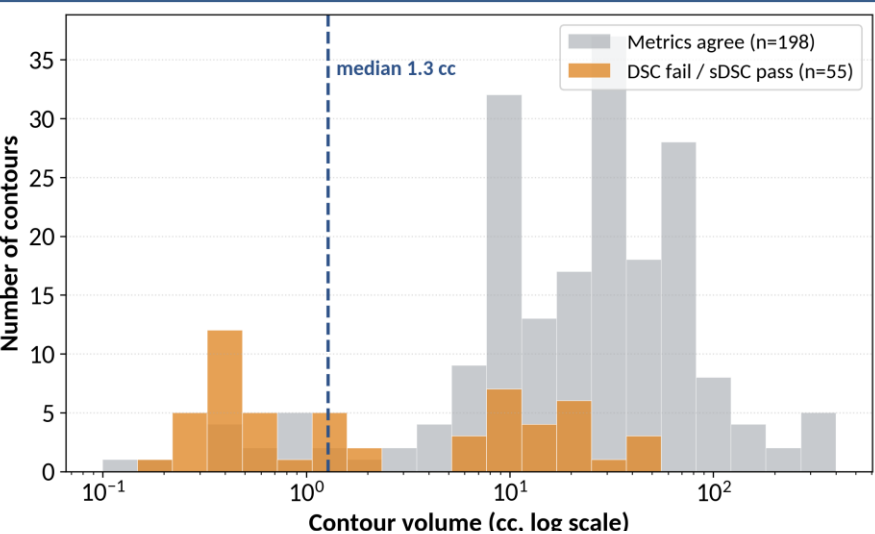


Figure 2 Contour volume for cases where DSC and surface DSC disagreed compared with cases where the two metrics agreed .The two metrics diverge specifically for small structures.

Table 2. Dosimetric impact of contours rejected by DSC (< 0.80) but accepted by surface DSC (≥ 0.85) — n = 55, volume < 10 cc.

Dosimetric endpoint	Median	IQR
Mean dose difference	0.15 Gy (2.8%)	0.01–0.99 Gy
Near-max (D2) difference	0.09 Gy (1.1%)	0.02–0.93 Gy

Conclusion

MVision AI produced clinically acceptable contours for most organs at risk across both head-and-neck and prostate sites. DSC disproportionately penalises small-volume contours, rejecting geometry that is dosimetrically acceptable. Surface DSC should therefore be the preferred acceptance metric for small OARs [2].

References

- Nikolov S, Blackwell S, Zverovitch A, Mendes R, Livne M, De Fauw J, et al. Clinically applicable segmentation of head and neck anatomy for radiotherapy: deep learning algorithm development and validation study. J Med Internet Res. 2021;23(7):e26151.
- Vaassen F, Hazelaar C, Vaniqui A, Gooding M, van der Heyden B, Canters R, et al. Evaluation of measures for assessing time-saving of automatic organ-at-risk segmentation in radiotherapy. Phys Imaging Radiat Oncol. 2020;13:1–6.